

# **Viologen-Functionalized Monolayers in Nanopores of Anodic Aluminum Oxide for Reagentless Multiplexed Biosensing**

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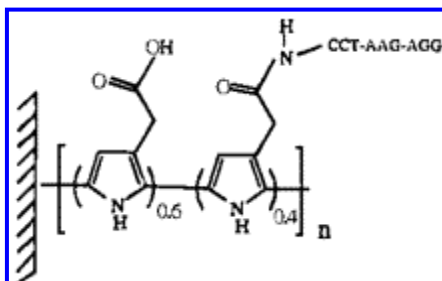
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## **OUTLINE**

- I. Formation of Viologen-Functionalized Monolayers on Bulky Gold for Reagentless Biosensing**
- II. Fabrication of Anodic Aluminum Oxide (AAO)**
- III. Formation of Viologen-Functionalized Monolayers in AAO for Reagentless Multiplexed Biosensing**

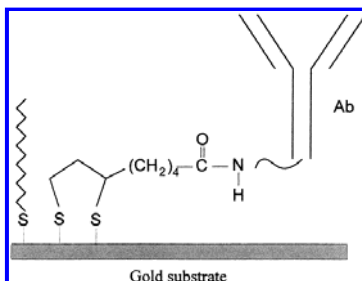
# *Direct Transduction of Biorecognition on Surfaces*

- **Direct Transduction Modes**
  - ◆ mechano-acoustic
  - ◆ surface plasmon resonance & fluorescence
  - ◆ piezoelectric & electrochemical
- **Electrochemical Transduction**
  - ◆ excellent for interfacing, at the molecular level, biorecognition events & electronic signal transduction processes.
  - ◆ uniquely qualified for meeting the size, cost, low-volume, and power requirements of decentralized testing.



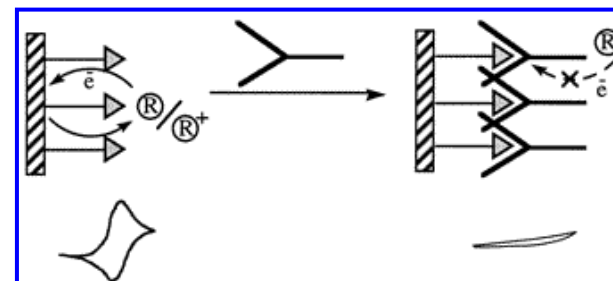
*J. Am. Chem. Soc.* **1997**,  
**119**, 7386.

Low interaction efficiency



*Anal. Chem.* **1997**,  
**69**, 3651.

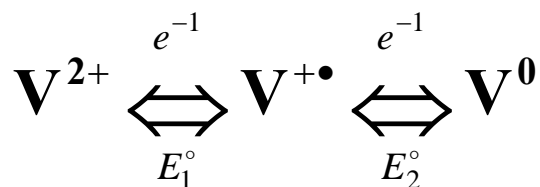
Small signal



*Angew. Chem. Int. Ed.* **2000**,  
**39**, 1180.

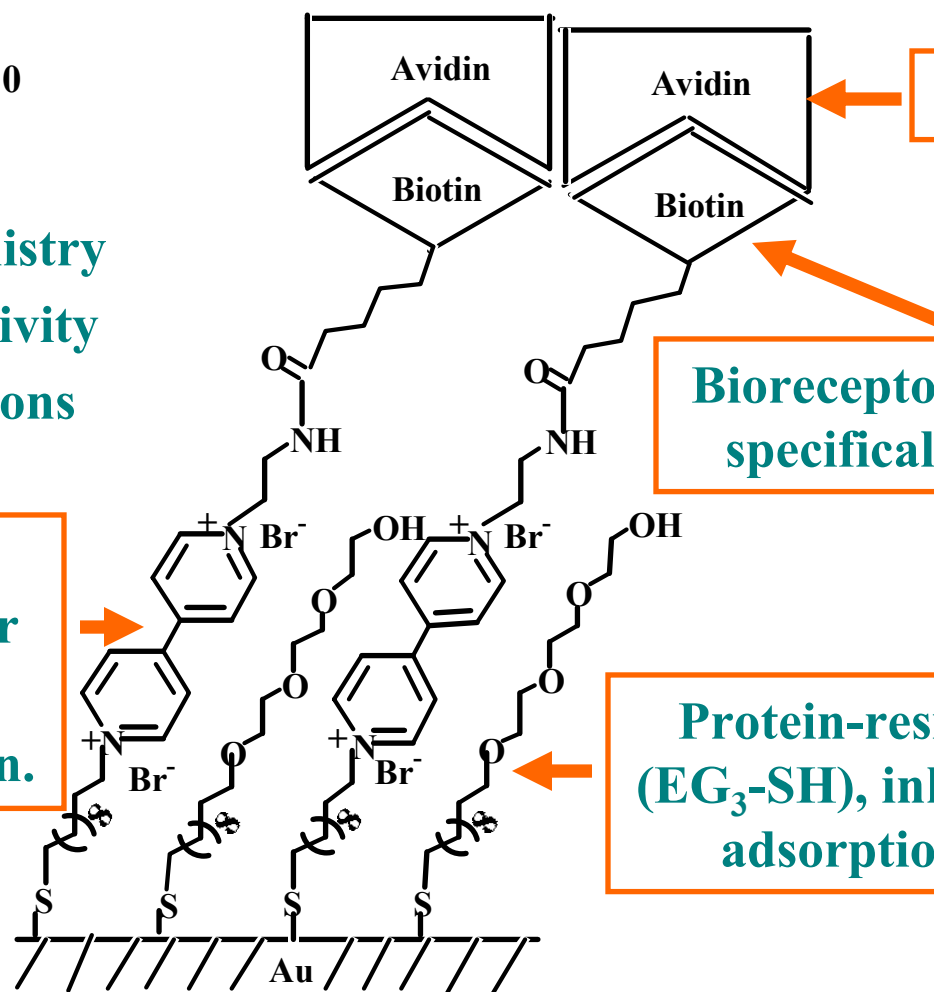
Low reproducibility

# Modular Molecular Assemblies



- excellent redox chemistry
- environmental sensitivity
- widespread applications

Electroactive species (viologen), change their redox properties as avidin is bound to biotin.



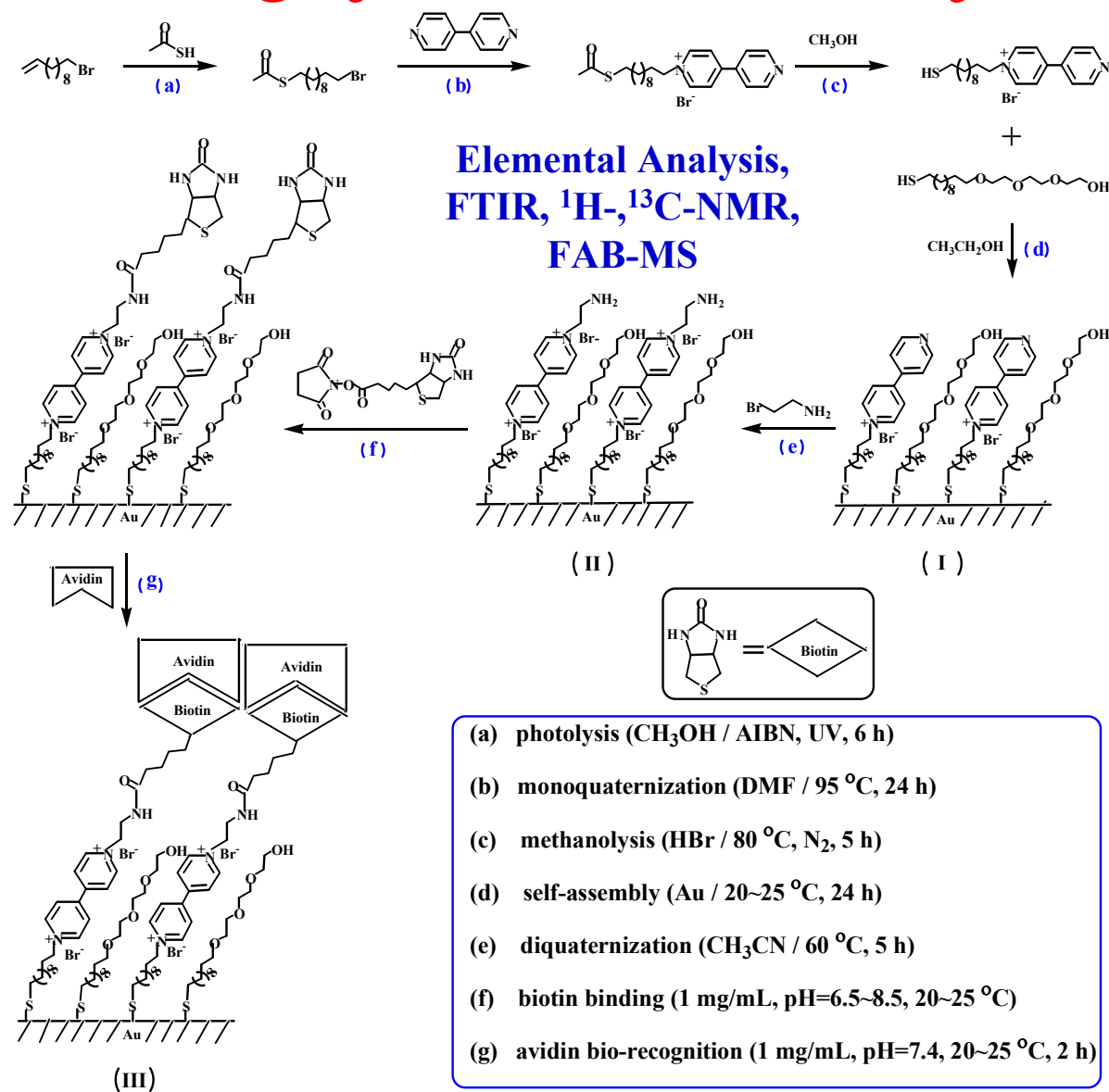
Targets (avidin)

Bioreceptors (biotin), bind specifically with avidin.

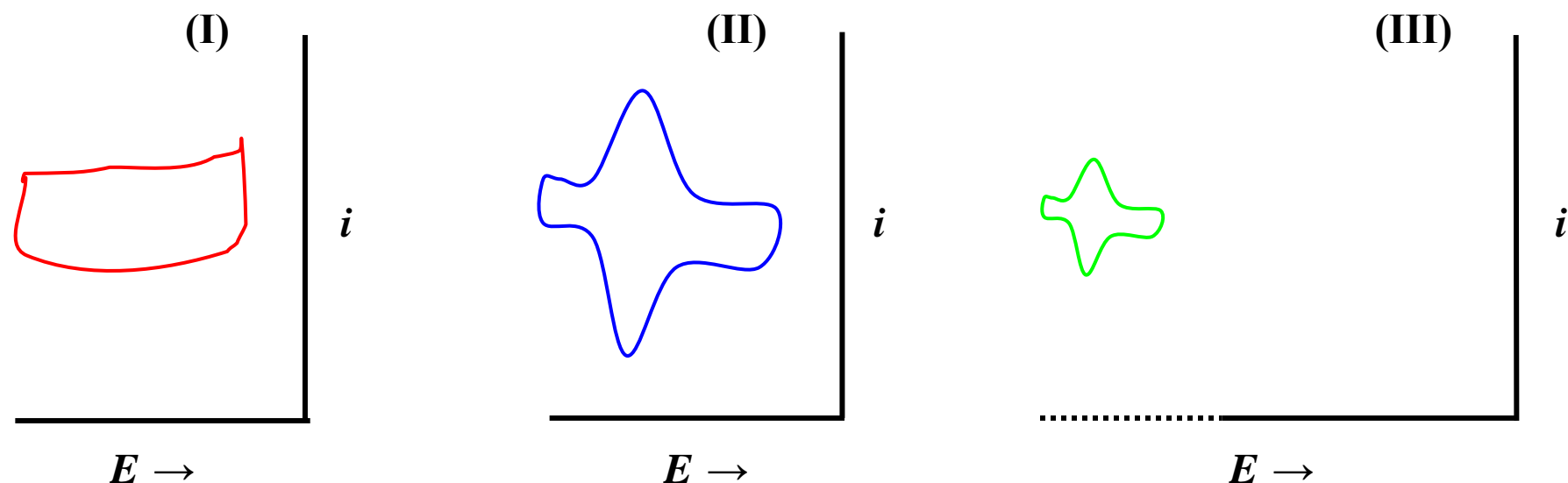
Protein-resistant moieties (EG<sub>3</sub>-SH), inhibit nonspecific adsorption of protein.

**Solution-phase organic synthesis of the transducer molecule with sulfhydryl, viologen and biotin groups is nearly impossible.**

# Scheme 1. Synthetic Path, Surface Reactions and Binding of Avidin to the Surface.



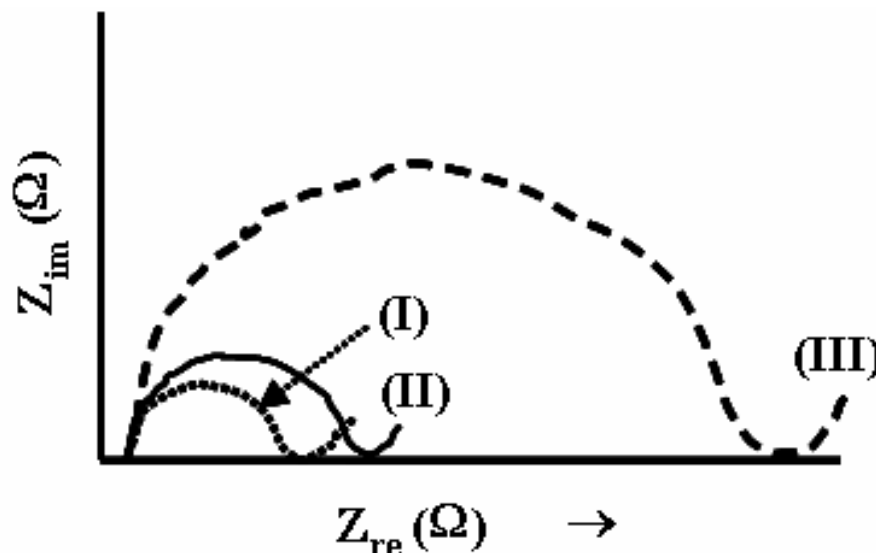
# *Cyclic Voltammetric Transduction*



*Scheme 2. Schematic Cyclic Voltammograms of the SAMs of (I), (II) and (III) in a Supporting Electrolyte.*

**Transduction is based on the change in the electrochemical properties of the surface-confined viologen groups.**

## *Electrochemical Impedance Spectroscopic Transduction*



*Scheme 3. Schematic Nyquist plots of the Faraday impedance spectra of the SAMs of (I), (II) and (III).*

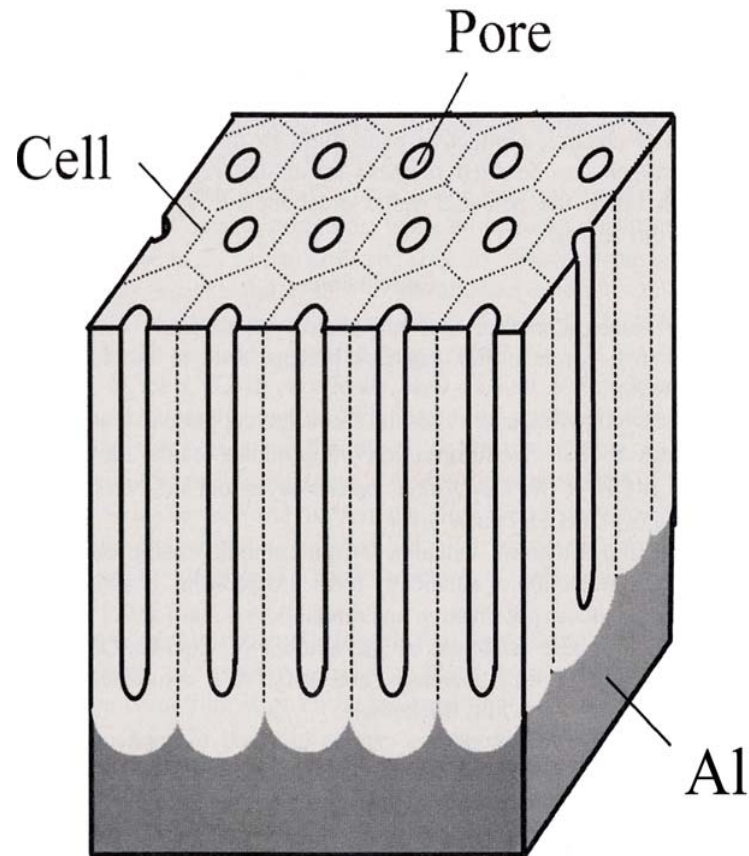
Transduction is based on the change in the electron transfer resistance ( $R_{ct}$ ) between the electrode and the redox markers in solution.

If more than one ligands are attached to the surface, it is possible to detect and quantify multi-analytes simultaneously.

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# *Idealized Structure of AAO*



(Masuda, H., et al,  
*Science* 1995, 268, 1466)



# *Properties and Applications of AAO*

## **Tunable pore features**

- diameter (10 - 300 nm)
- density ( $10^8 - 10^{12} \text{ cm}^{-2}$ )
- spacing (30 - 500 nm)
- depth (up to hundreds of  $\mu\text{m}$ )

## **Specific advantages**

- structural variability
- optical transparency
- excellent stability
- excellent dielectric properties
- low cost and high throughput
- potential for large-scale production

## **Potential applications**

- nanotemplates
- etch masks
- microfluidic devices
- base materials
- MEMS
- bio-supports
- 2D photonic crystals
- ultra-filtration membranes
- micro-engineered catalysts
- magnetic memory arrays

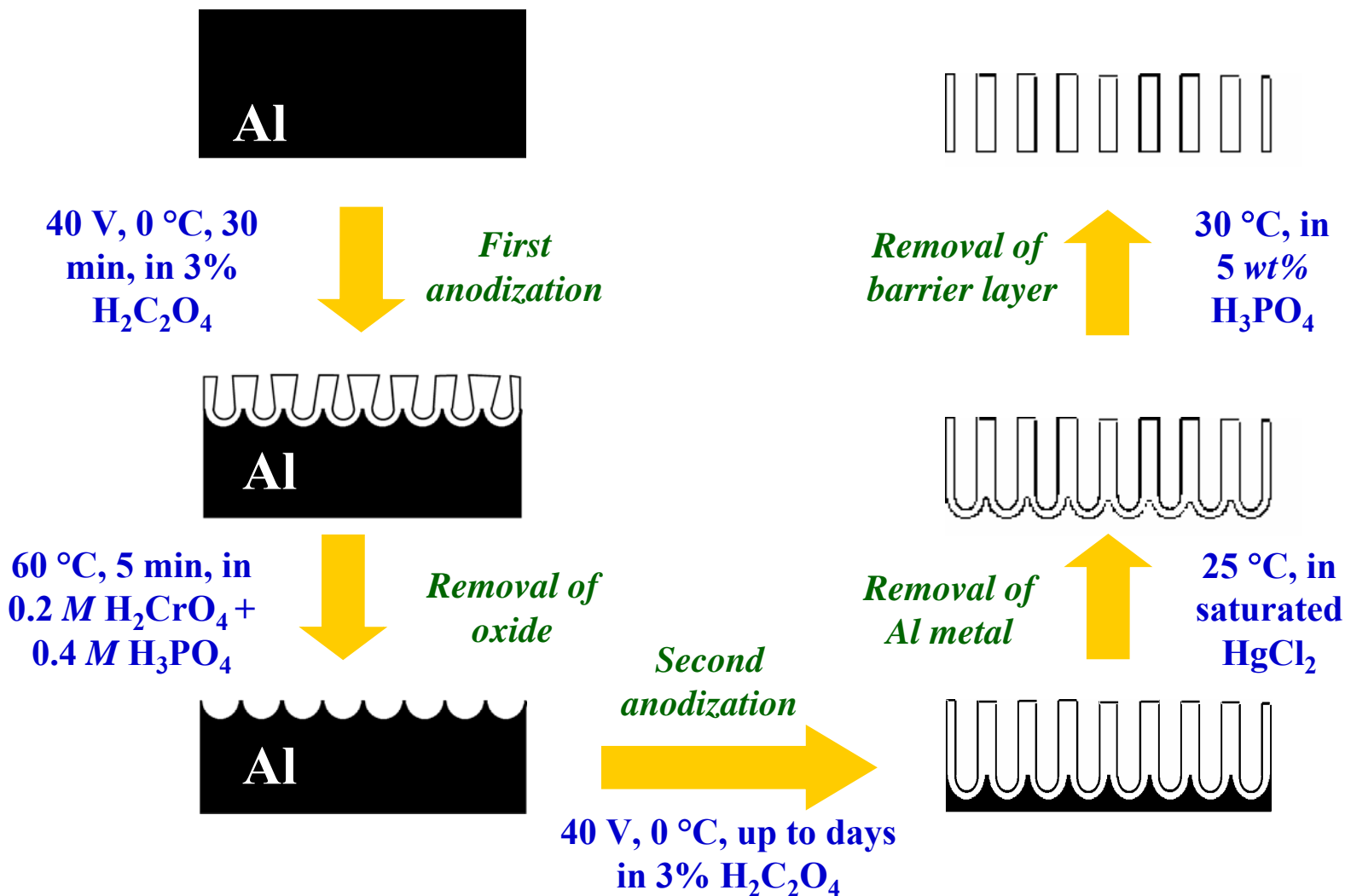
## *Fabrication of AAO*

At a constant low temperature and in an appropriate acidic electrolyte, NAA grow through galvanostatic or potentiostatic anodization of aluminum (5N). This process is rapid, inexpensive, reproducible, and controllable.

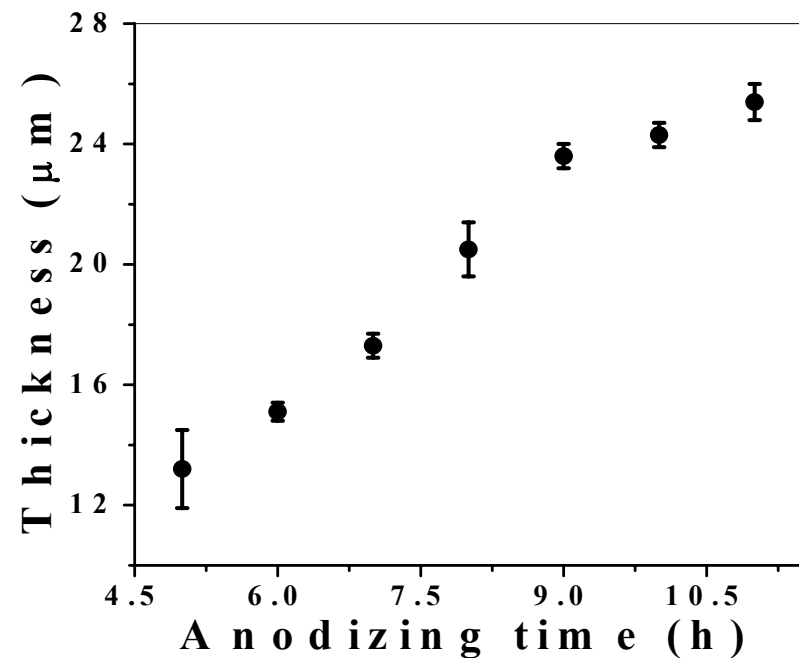
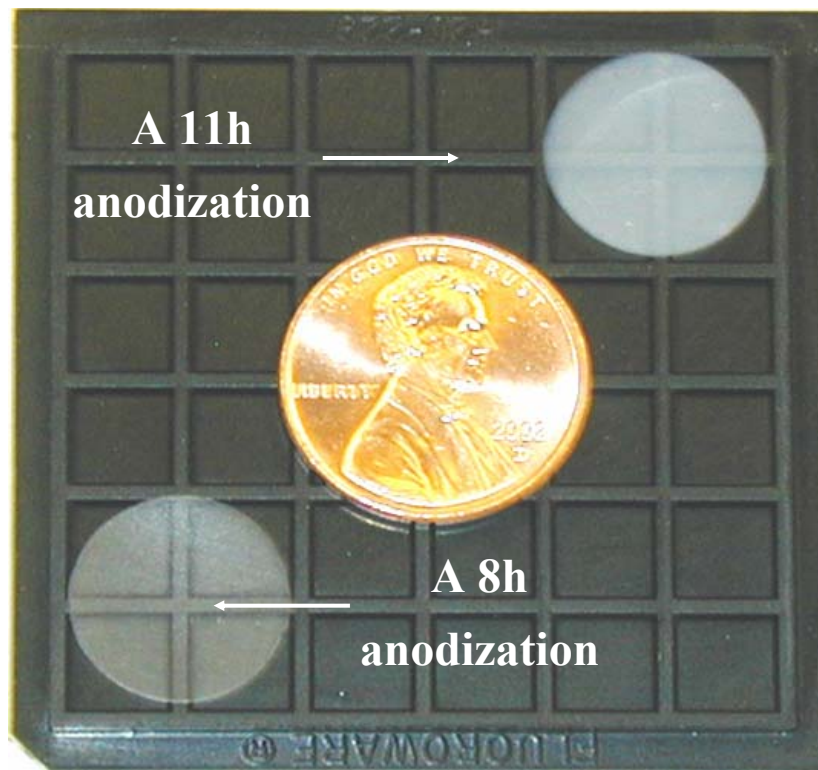
### *Optimized Anodization Parameters*

Electrolyte	Temp. (°C)	Voltage (V)	Diameter (nm)
1.2 M H <sub>2</sub> SO <sub>4</sub>	1	19	15
0.3 M H <sub>2</sub> SO <sub>4</sub>	1	26	20
0.5 M H <sub>2</sub> SO <sub>4</sub>	0	25	30
0.3 M H <sub>2</sub> C <sub>2</sub> O <sub>4</sub>	14	40	40
0.3 M H <sub>2</sub> C <sub>2</sub> O <sub>4</sub>	10	40	45
0.3 M H <sub>2</sub> C <sub>2</sub> O <sub>4</sub>	14	60	60
1.0 M H <sub>3</sub> PO <sub>4</sub>	3	95	90
1.0 M H <sub>3</sub> PO <sub>4</sub>	0	160	400

# *Two-Step Anodization Process and Post-Treatments*

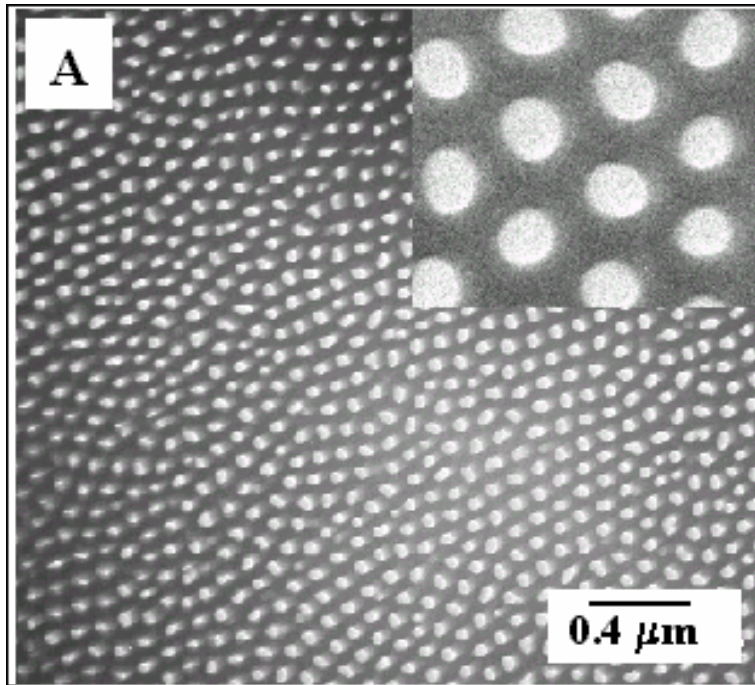


# *Dependence of the Membrane Thickness of AAO on Anodization Time*

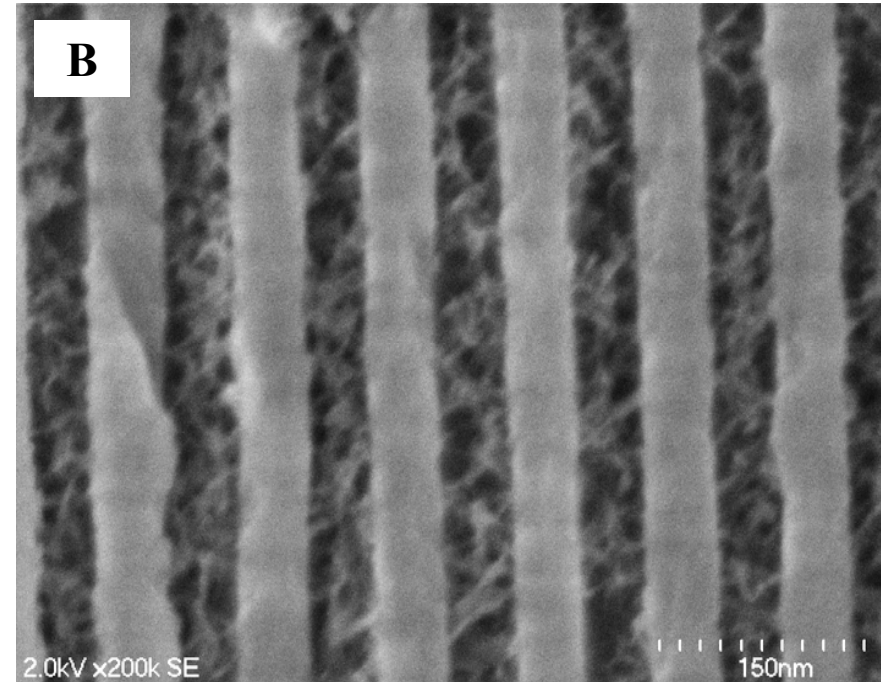


(Yan, J., et al,  
*Adv. Mater.* 2003, 15, 2015)

# *Electron Micrographs of the Freestanding, Through-Hole AAO Membranes*



**Plan view (TEM)**



**Cross-sectional view (SEM)**

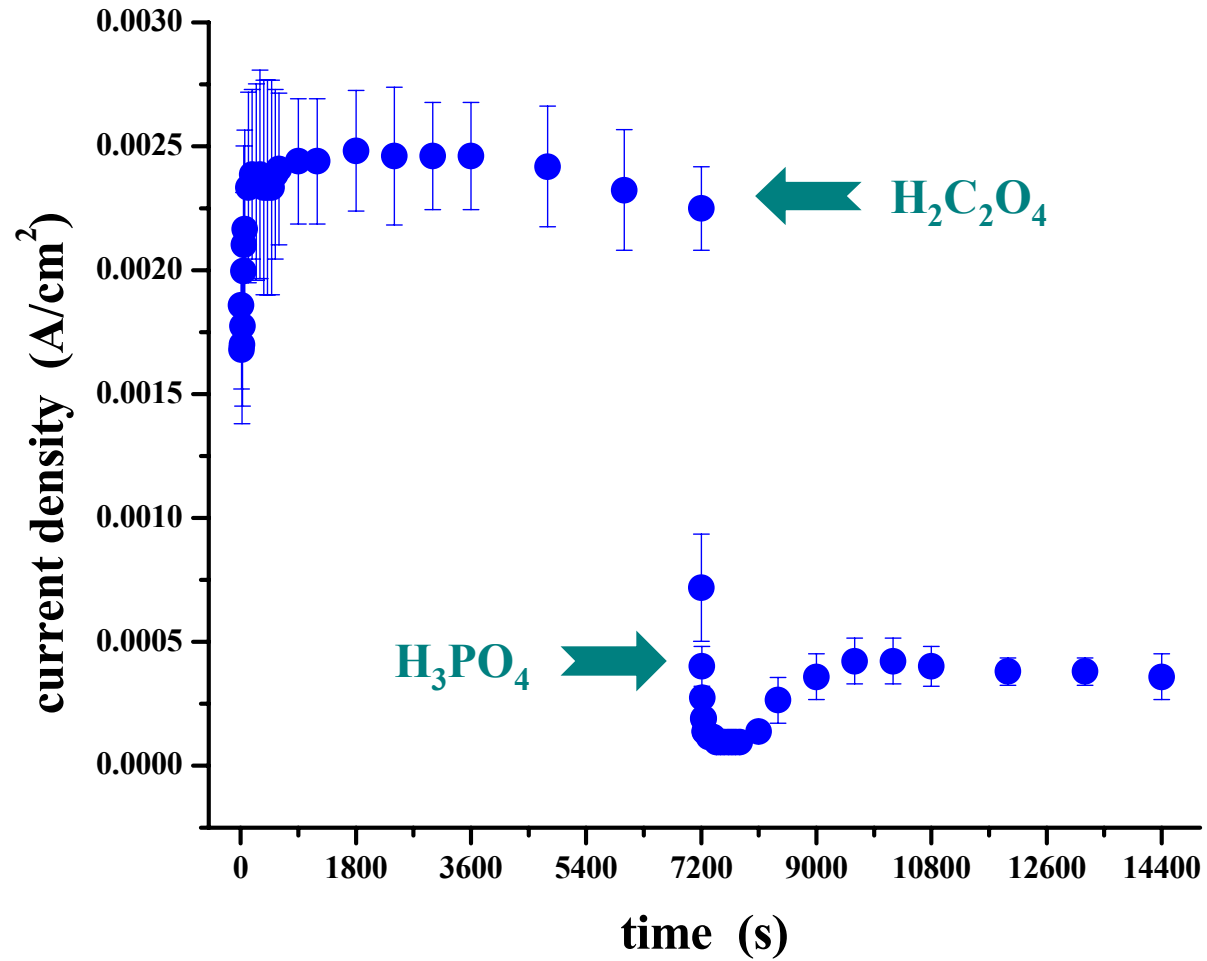
**Pore Diameter:  $(45 \pm 2)$  nm; Pore Depth:  $\sim 10$  μm; Pore Density:  $1.7 \times 10^{10}$  cm<sup>-2</sup>.**

**(Yan, J., et al, *Encyclopedia of Nanoscience and Nanotechnology*, Schwarz, J.; et al, Eds.; 2004, 83)**

# *Motivations for Design of Interconnected AAO*

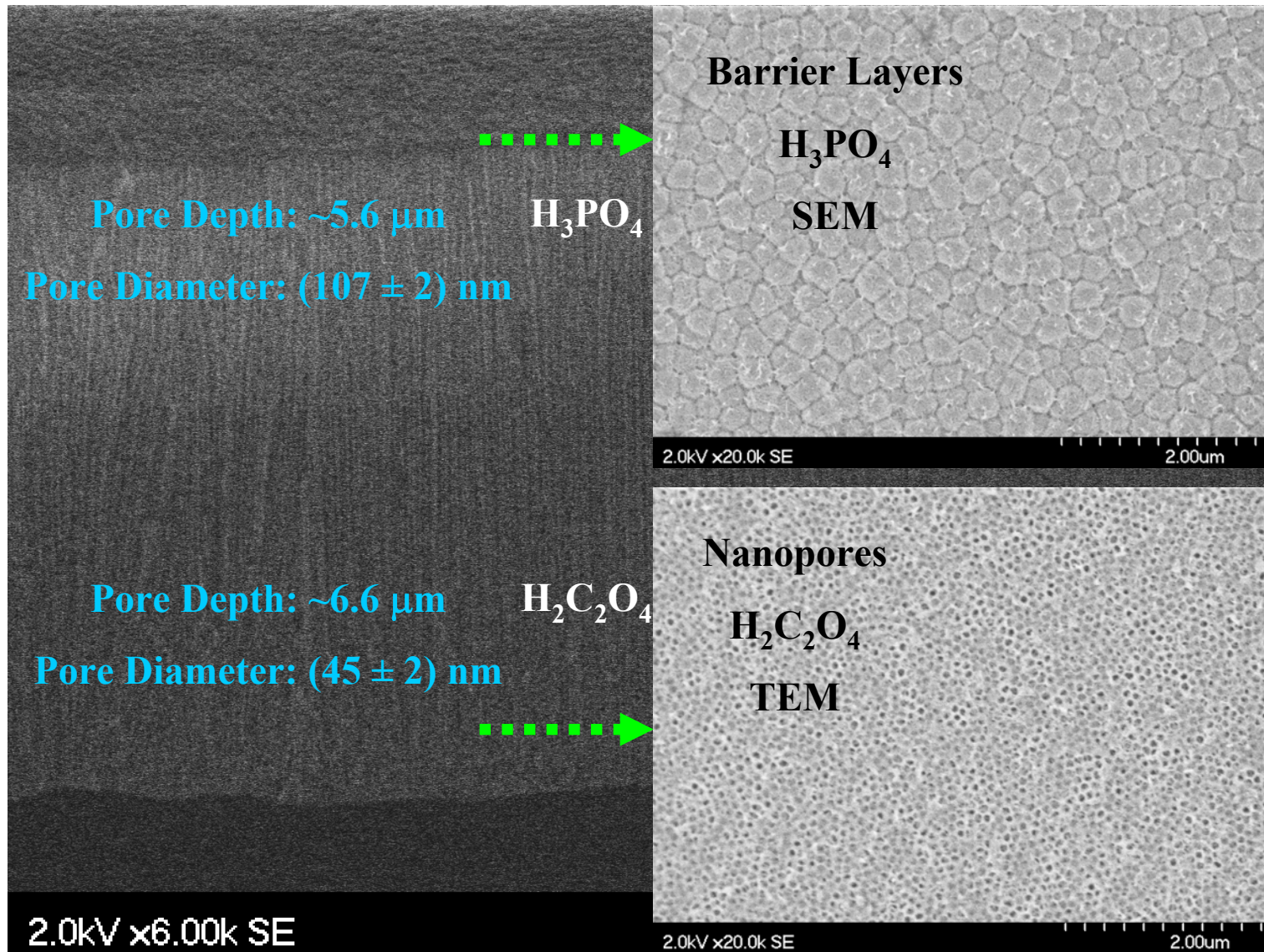
- The fabrication of rationally designed, interconnected, nanotubes is vital to the development of nanotube electronics and biotechnologies. However, this is difficult to achieve using conventional processes (*e.g., laser ablation, CVD, etc.*), which lack a high degree of control in the fabrication and in the properties of the products.
- Various postgrowth methods have been reported, but they have been hard to implement and have been subject to defects.
- Controlled anodization of ultra-pure aluminum has recently been demonstrated to have the potential of fabricating interconnected, ordered AAO.

# *Current Density - Time Plot*



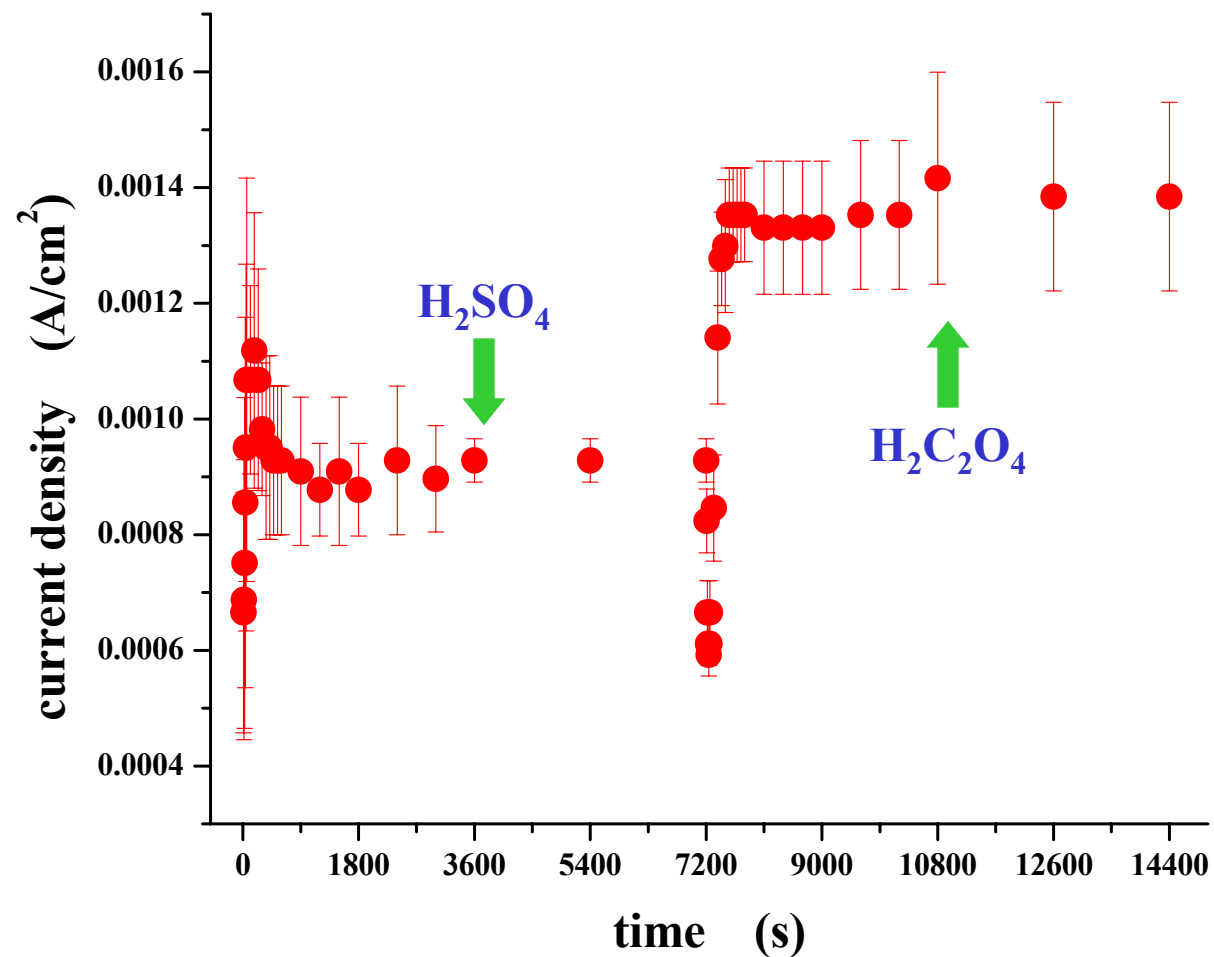


# *Scanning Electron Micrographs of the Freestanding, Merged AAO*





# *Switching Electrolytes Between Sulfuric and Oxalic Acids*



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# *Motivations for Forming Viologen-Functionalized Monolayers in AAO*

- Identification & Quantitation of Biomolecules in Mixtures
  - ◆ Separation (e.g., gel electrophoresis & mass spectrometry)
    - low throughput; lack of quantitation; high cost per assay.
  - ◆ Through specific binding with a receptor molecule (e.g., commercially available DNA micro-arrays)
    - not widely available for DNA-protein, protein-protein, & protein-ligand bindings; require fluorescent labels.
- The modification of nanotubes with biorecognition elements imparts high-sensitivity and high-throughput onto devices based on 1-D nanostructured materials. This allows individual functionalizations, enables reagentless multiplexed binding assays for large mixtures of biomolecules, and offers novel opportunities of assembling nanosensors into functional integrated devices.

## *Conclusions & Future Work*

- Combining a 3-step synthesis of a precursor with its subsequent surface derivatizations, we are expecting to produce the complex transducer molecule in higher purity and yield than would be possible with solution phase synthesis.
- Tunable, interconnected nanoporous AAO can be easily fabricated in large quantities by switching the electrolytes and adjusting the voltages accordingly.
- Our future work will be centered on: (1) attaching multiple ligands to the surface for simultaneous detection and quantitation of various affinity receptors; and (2) creating nanosensor arrays for parallel real-time monitoring of multiple analytes.

## ***Acknowledgement***

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**Ms. Laxmi Chinnam**                      **Ms. Elizabeth Hawkins\***  
**Ms. Ashakiran Parvathaneni**              **Mr. Roger Williams\***  
**Mr. Karthik Gade**                      **(\*undergraduate students)**